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# A pH-responsive ZIF-8-encapsulation Au nanocluster fluorescent probe applying for convenient and efficient detection of glucose

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## ABSTRACT

Glucose plays a crucial role in maintaining human health as an indispensable source of energy in living organisms. Accurate monitoring of glucose levels in living organisms and detecting it in food is essential. In this study, gold nanoclusters (AuNCs) with unique aggregation-induced emission (AIE) effects were encapsulated within zeolite imidazole framework (ZIF-8) to fabricate a pH-responsive AuNCs@ZIF-8 fluorescent nanocomposite. The fluorescence intensity had significant sevenfold enhancement compared to AuNCs alone due to the structural domain-limiting effects exerted by ZIF-8, which effectively inhibited the rotations and vibrations of the AuNCs ligands. Based on the increased acidity generated by glucose catalytic oxidation *via* glucose oxidase (GOx), the subsequent degradation of ZIF-8 structure and the consequent reduction of AuNCs with AIE effects were achieved, and a rapid and efficient fluorescence quantification for glucose was performed. The constructed AuNCs@ZIF-8-based fluorescent probe demonstrated a favorable linear response to glucose, achieving a detection limit of 0.096 mmol/L and providing a rapid and efficient approach suitable for assessing glucose levels in both blood and beverage samples.

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## 1. Introduction

Glucose oxidation, a fundamental metabolic process in living organisms, holds immense importance in supplying energy to biological cells and supporting various physiological functions<sup>[1-2]</sup>. Blood glucose levels serve as a critical indicator of human health status, typically falling within the range of 3.9–6.0 mmol/L when measured in a fasting state<sup>[3]</sup>. Deviations from these normal levels can lead to a variety of health problems, such as hypoglycemia, cardiovascular disease, diabetes, and associated complications, posing significant risks to individual health<sup>[4-5]</sup>. In addition, glucose is a vital

additive ingredient in food fields and commonly incorporated to enhance the taste and quality of food products, especially in glucose-containing beverages<sup>[6]</sup>. Over consumption of glucose can adversely affect organs such as the liver and kidneys and disrupt normal physiological functions<sup>[7]</sup>. Therefore, it is imperative to develop rapid, convenient, and efficient strategies for the surveillance and quantitation of glucose levels in blood and food to maintain human health and food safety.

Up to this point, a variety of analytical methods based on different principles have been explored and applied for detecting glucose targets in clinical samples or food testing processes. These methods encompassed techniques such as high-performance liquid chromatography (HPLC) for chromatographic separation<sup>[8]</sup>, surface-enhanced Raman scattering (SERS) employing noble metals<sup>[9]</sup>,

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electrochemical analysis<sup>[10–11]</sup>, fluorescence and colorimetric<sup>[12]</sup>. Among the array of techniques utilized for detecting glucose targets in clinical samples or food testing, fluorescence sensing analysis strategies have attracted significant attention owing to their sensitivity, operational simplicity, and cost-effectiveness. Considering that glucose does not have naturally fluorescence due to its small molecular size, enzymatic catalysis is commonly required to generate specific substances for detection. Glucose oxidase (GOx) has become the enzyme of choice for glucose detection, favored for its robust activity, remarkable specificity, and cost-effectiveness. Most of the prevailing glucose sensing strategies involved immobilizing GOx on the sensing interface and quantifying the amount of H<sub>2</sub>O<sub>2</sub> produced through its catalytic action of glucose substrates to facilitate glucose detection<sup>[13–14]</sup>. Sun et al.<sup>[15]</sup> reported an ultrasensitive fluorescent biosensor to be used for glucose detection based on a Fenton-like reaction triggered chemical redox-cycling signal amplification strategy, with a limit of detection (LOD) of 0.3 nmol/L. Therefore, it can provide a strategy for developing low-cost and sensitive methods for biological and clinical diagnostics applications<sup>[16]</sup>. However, the immobilization of GOx at the sensing interface is prone to deactivation during prolonged storage, potentially compromising assay sensitivity and resulting in inaccurate results. Therefore, there is significant research value in creating a novel and efficient fluorescence sensing strategy for glucose that aimed at improving the convenience, sensitivity, and stability of glucose detection methods.

As a class of ideal fluorescent nanomaterials, metal nanoclusters (MNCs) such as Au, Ag, Cu, have attracted increasing interest. The luminescence performance of MNCs can generally be improved through strategies such as fluorescence resonance energy transfer (FRET), antenna effect (AE) and aggregation-induced emission (AIE), etc., among which the AIE effect is gradually becoming a research hotspot. Wang et al.<sup>[17]</sup> found the fluorescence intensity of copper nanoclusters (CuNCs) is enhanced strongly through the glutathione (GSH)-controlled AIE enhancement of self-assembled CuNCs. Wang et al.<sup>[18]</sup> reported a kind of specific structure of self-assembled CuNCs, greatly enhancing the fluorescence emission intensity of tetracycline (TC). Inspired by these reports, the application of the AIE-type gold nanoclusters (AuNCs) composite materials were investigated. The AuNCs, among various MNCs, have great application prospects in various fields such as bioimaging, optical sensing and nanocatalysis by virtue of their more excellent stability<sup>[19–21]</sup>. Despite the AuNCs effectively overcoming aggregation-caused quenching (ACQ), a common issue with conventional organic luminescent materials, their lower fluorescence quantum yield (QY) has largely restricted their broad application. The AIE effects are a typical photophysical phenomenon, and weakly fluorescent or non-fluorescent materials exhibit specific fluorescence enhancement when in an aggregated state due to the restriction of molecules (or ligands) motion<sup>[22]</sup>. This unique and controllable effects have been applied to enhance the fluorescence intensity of certain nanomaterials, thus expanding their range of applications in fluorescence-based technologies. Synthesizing with thiolate ligands and utilizing GSH as a reductant and stabilizer, AuNCs demonstrated a typical core-shell structure and AIE properties. When aggregated, the intramolecular vibrations and rotations of the surface ligands are restricted, thus suppressing the non-radiative transition of the excited state associated with the ligands, resulting in pronounced fluorescence

enhancement<sup>[23]</sup>. Moreover, synthesizing AIE-type AuNCs is straightforward and controllable, making it an effective strategy for producing AuNCs material with tunable fluorescence intensity<sup>[24]</sup>.

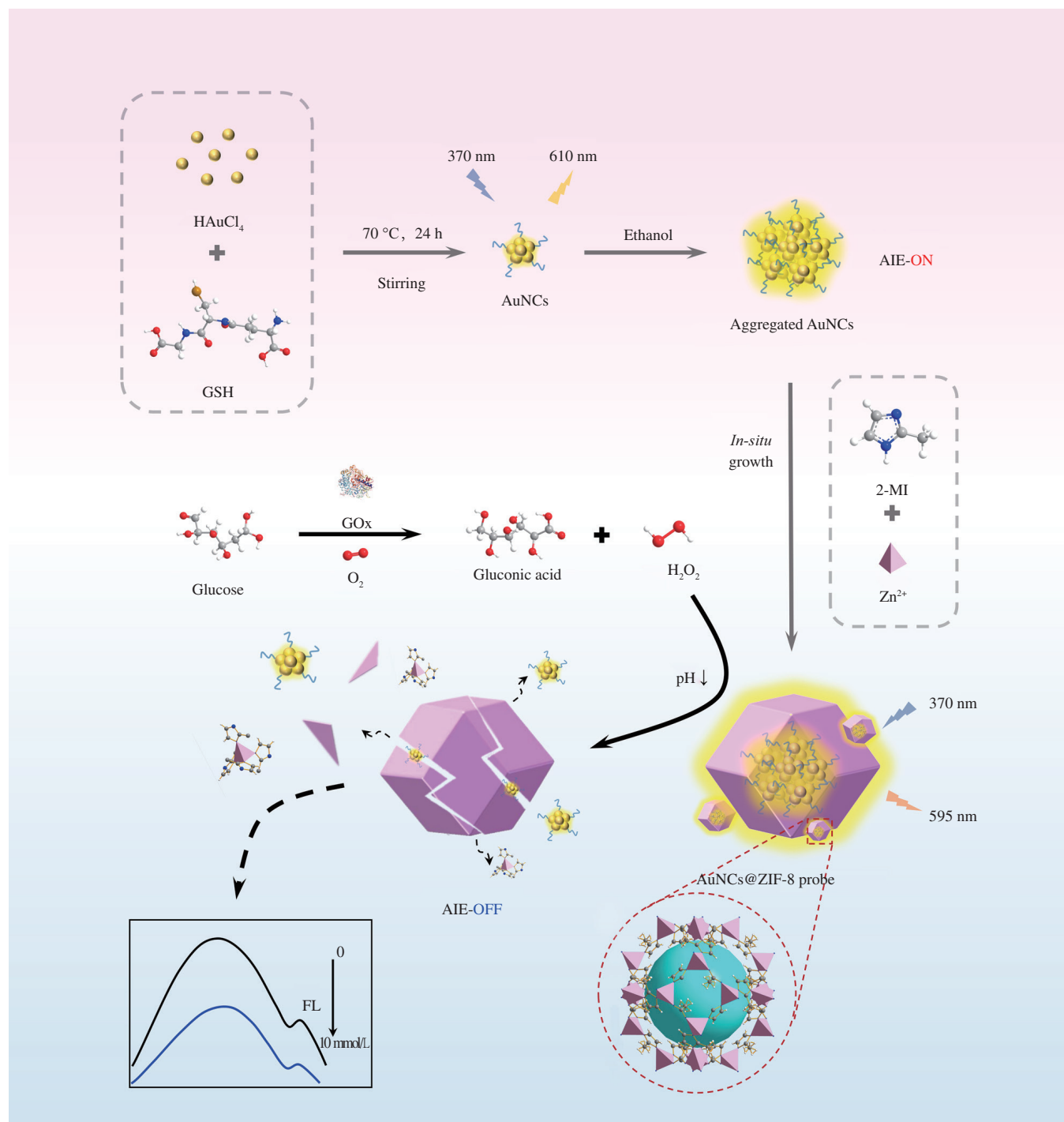
Metal-organic frameworks (MOFs) are a class of materials assembled from specific metal ions and organic ligands, showcasing characteristics such as orderly pore structures, high loading capacities, and exceptional stability<sup>[25]</sup>. Zeolite imidazole framework (ZIF-8), a type of MOFs, has attracted considerable attention due to its simple preparation process, high porosity, and sensitive response to pH values<sup>[26]</sup>. It is promising for various applications in adsorption, curing, and encapsulation of small-molecule targets, biological proteins, and others. Benefiting from the high porosity of MOFs, AIE luminogens (AIEgens) or nanomaterials with AIE characteristics can be encapsulated as guests into MOFs. Leveraging the excellent luminescent properties of AIE materials and the unique hollow structure of MOFs, hydrogen bonds or coordination bonds can be formed with guest molecules to influence fluorescence emission, facilitating the quantitative detection of target analytes. For instance, Xie et al.<sup>[27]</sup> successfully synthesized luminescent metal-organic frameworks (LMOFs) by incorporating AIEgens into ZIF-8, enhancing the fluorescence emission efficiency while retaining the AIE characteristics. They developed a fluorescent colorimetric paper strip utilizing LMOF-2 with GOx for visual detection of glucose in serums. This method demonstrated outstanding performance within the normal fasting blood glucose range of 3–8 mmol/L, offering a novel solution for glucose monitoring. Hence, by exploiting the domain-limiting effects of the ZIF-8 framework, the induced aggregation of AuNCs significantly enhanced the fluorescence efficiency and effectively improved self-capability to resist external environmental interference, thereby improving fluorescence stability and laying the groundwork for the development of fluorescence analysis strategies<sup>[28–29]</sup>.

In this study, a fluorescent strategy for detecting glucose targets was introduced by encapsulating AIE-type AuNCs within the ZIF-8 structure (Fig. 1). ZIF-8 underwent self-assembled around the aggregated AuNCs, resulting in a significant enhancement in their fluorescence emission efficiency. Upon GOx catalysis of glucose targets and subsequent alterations in environmental acidity, protonation of the methylimidazole ligands linkers in ZIF-8 occurred, disrupting the coordination with Zn<sup>2+</sup> ions and leading to the decomposition of the framework<sup>[30]</sup>. The ZIF-8 framework decomposed and removed the aggregation effects of AuNCs, thus enabling rapid and efficient detection of glucose targets.

## 2. Material and methods

### 2.1 Reagents and materials

Glucose (99.7%), sucrose (99.7%), and *L*-ascorbic acid (99.7%) were purchased from Tianjin Chemical Reagent No.1 Factory (Tianjin, China). GSH (98.0%), *D*-xylose (99.0%), *D*-galactose and *D*-maltose monohydrate (98.0%) were procured from Soleibao Technology Co., Ltd. (Beijing, China). GOx (180 U/mg) and 1*H*-purine-2,6,8(3*H*,7*H*,9*H*)-trione (98.0%) from *Aspergillus niger* were obtained from Aladdin Chemical Reagent Co., Ltd. (Shanghai, China). *L*-Cysteine (99.0%), *D*-serine (98.5%), gold (III) chloride trihydrate (HAuCl<sub>4</sub>·3H<sub>2</sub>O, 99.9%) and 2-methylimidazole (2-MI, 99.0%)



**Fig. 1** Schematic diagram of preparation of AuNCs@ZIF-8 fluorescent probe for glucose fluorescence detection.

was received from Macklin Biochemical Co., Ltd. (Shanghai, China). The reagents methanol, ethanol, zinc nitrate hexahydrate ( $\text{Zn}(\text{NO}_3)_2 \cdot 6\text{H}_2\text{O}$ , 99.0%), and hydrogen peroxide ( $\text{H}_2\text{O}_2$ , 30.0%) were purchased from Sinopharm Chemical Reagent Co., Ltd. (Shanghai, China). Ultrapure water was produced using a Milli-Q Purification System (18 M $\Omega$ ·cm, Millipore, USA).

## 2.2 Instrumentation

The structures and morphologies of AuNCs, ZIF-8, and AuNCs@ZIF-8 were characterized by transmission electron microscopy (TEM, Talos G2 200X, Thermo, USA) and scanning electron microscopy (SEM, Apreo, Thermo, USA). The crystal surfaces of the materials were characterized using an X-ray diffractometer (XRD, D8 Advance, Bruker, Germany) within a  $2\theta$  range of 5°–90° and a scanning speed

of 5°/min. The composition and valence states of AuNCs@ZIF-8 were studied using X-ray photoelectron spectroscopy (XPS) obtained by Scientific EscaLab 250Xi (Thermo, USA). Fourier transform infrared spectroscopy (FT-IR) spectra were obtained using a Nicolet iS50 spectrometer (Thermo, USA). The specific surface area was determined by N<sub>2</sub> adsorption at 77 K using a BELSORP-max II instrument (Microtrac BEL, Japan). Thermogravimetric analyzer (TGA, Q50, TA, USA) was employed to verify the stability and composition of the fluorescent probe. Ultraviolet-visible (UV-vis) spectra and fluorescence spectra were recorded using an ultraviolet spectrophotometer (UV-2600, Shimadzu, Japan) and a fluorescence spectrophotometer (Lumina, Thermo, USA).

### 2.3 Synthesis of the AIE-type AuNCs

The AIE-type AuNCs utilized in this work were synthesized through the reduction of HAuCl<sub>4</sub> using GSH. Specifically, 1.0 mL of HAuCl<sub>4</sub> (18 mmol/L) and 0.3 mL of GSH (100 mmol/L) were mixed in ultrapure water. As the solution's color shifted from a light yellow to transparent, the volume was adjusted to 10.0 mL with ultrapure water. Subsequently, the solution was heated to 70 °C, away from light, and gently stirred for 24 h. The resulting light-yellow solution containing the AIE-type AuNCs was then stored in the dark at 4 °C for subsequent use.

### 2.4 Preparation of AuNCs@ZIF-8 nanocomposite

The preparation of the AuNCs@ZIF-8 nanocomposite involved the *in-situ* synthesis of ZIF-8 around the AIE-type AuNCs. Initially, 4.0 mL of the prepared AuNCs solution was mixed with an equal volume of ethanol, and centrifuged at 10 000 r/min for 15 min. The resulting precipitated AuNCs were re-dispersed in 2.0 mL of methanol, followed by the addition of 10.0 mL of Zn(NO<sub>3</sub>)<sub>2</sub>·6H<sub>2</sub>O (30 mmol/L) and 10.0 mL of 2-MI (90 mmol/L). The mixture was subjected to magnetic stirring for 5 min and subsequently sonicated for 40 min avoiding light. Finally, the solid product was collected by centrifugation, thoroughly washed with methanol, freeze-dried, and stored in the dark at 4 °C for subsequent use.

### 2.5 Fluorescent probe based AuNCs@ZIF-8 for glucose detection

The fluorescence detection process of the glucose targets using the prepared AuNCs@ZIF-8 probe involved the following steps: 75 µL of glucose working solutions at concentrations ranging from 1 to 10 mmol/L were accurately prepared and thoroughly mixed with 25 µL of GOx (2.7 U) and 100 µL of PBS (10 mmol/L, pH 6.5). A total of 50 µL of the prepared AuNCs@ZIF-8 solution (5 mg/mL) was added to the aforementioned reaction system, which was then diluted to a total volume of 500 µL using ultrapure water. The entire system was then subjected to incubation in a 37 °C water bath for 30 min. Subsequently, the fluorescence spectrum of the resulting solution system were analyzed and the fluorescence maxima at wavelength from 500 to 700 nm were recorded for the calculation of glucose contents. The LOD was determined based on the slope (*k*) of the calibration curve obtained from the fluorescence response of the AuNCs@ZIF-8 probe to various concentrations of glucose. It was

calculated using the formula  $3\sigma/k$ , where  $\sigma$  represents the standard deviation of the blank and  $k$  represents the slope of the calibration curve.

### 2.6 Analysis of glucose in real samples

To assess the practical utility of the prepared AuNCs@ZIF-8 probe in glucose measurement, fresh blood samples obtained from healthy volunteers and commercially available glucose beverages were employed as real samples for fluorescence detection. The sample measurement process was described as follows: 75 µL of either blood or beverage samples were accurately measured and subsequently centrifuged at 12 000 r/min for 10 min. The resulting supernatant from beverage samples underwent a 50-fold dilution with ultrapure water, while no further treatment was necessary for the supernatant of the blood samples. Then, 75 µL of the treated sample was mixed with 25 µL of GOx (2.7 U) and 100 µL PBS, followed by the addition of 50 µL of the prepared AuNCs@ZIF-8 solution (5 mg/mL) and 250 µL of ultrapure water for fluorescence analysis after incubation at 37 °C for 30 min. Three levels of glucose (1, 4, and 7 mmol/L) were added to each of the 3 beverage samples, and a prepared fluorescent probe was applied for glucose detection.

## 3. Results and discussions

### 3.1 Preparation of AuNCs@ZIF-8 probe and glucose detection principle

Fig. 1 presented the schematic diagram of the preparation and operational mechanism of the AuNCs@ZIF-8 probe. Initially, the AIE-type AuNCs were synthesized through the “one-pot method”, with GSH serving as both stabilizer and reductant. Subsequently, the dispersed AuNCs were induced to aggregate in the presence of the organic solvent ethanol, activating the AIE effects. The Zn<sup>2+</sup> ions interacted with –COO<sup>–</sup> groups on the ligands of AuNCs, which formed the ZIF-8 framework through interaction with the N atoms of 2-MI, facilitating the successful self-assembly of ZIF-8 around AuNCs. The confined space within the ZIF-8 structure restricted the distance between the AuNCs, enhancing the interactions of their surface groups, and limited the vibrations and rotations of the surface ligands, promoting further aggregation of AuNCs. This enhanced aggregation activated the energy transition from non-radiative to radiative, resulting in strong fluorescence emission from the AuNCs@ZIF-8 nanocomposite. Under acidic conditions, the protonation of methylimidazole ligands linkers occurred, disrupting the coordination between Zn<sup>2+</sup> ions and the imidazole rings, making the ZIF-8 structure sensitive to acidity. In the presence of oxygen, glucose molecule was catalytically decomposed by GOx into gluconic acid and H<sub>2</sub>O<sub>2</sub> (Eq. 1), consequently increasing the acidity in the microenvironment.



This heightened acidity can cause the breakdown of the ZIF-8 structure, leading to the release of internally confined AuNCs and a subsequent reduction in the fluorescence intensity of the system. Based on this decrease in fluorescence intensity, the quantitative analysis of glucose targets can be achieved.



### 3.2 Characterization of AIE-type AuNCs and AuNCs@ZIF-8 nanocomposite

TEM analysis showed that the resulting AIE-type AuNCs displayed a uniform spherical morphology, with an average diameter of approximately 1.57 nm (Figs. 2A and B). This ultra-small size promoted the formation of aggregated states, which endowed them with distinctive luminescent properties and a high QY. Additionally, the aggregation of presynthesized AuNCs were induced by ethanol, an undesired solvent. Subsequently, the self-assembly of ZIF-8 around the aggregated AuNCs was achieved through ultrasound-assisted precipitation, forming the AuNCs@ZIF-8 nanocomposite. As shown in Fig. S1, the colors of AuNCs in solution (visible: light-yellow; UV: orange) and initial ZIF-8 solid powder (visible: white; UV: blue) contrasted starkly with the AuNCs@ZIF-8 powder acquired subsequent to the embedding of AuNCs, which exhibited a light-yellow color under visible light and a distinct bright yellow color under UV irradiation. The morphological characteristics of ZIF-8 before and after being embedded in AuNCs were investigated using TEM and SEM. As illustrated in Figs. 2C, D and F, the crystal morphology of the synthesized AuNCs@ZIF-8 nanocomposite closely resembled that of pristine ZIF-8, with an average particle size maintained at approximately 132.6 nm. Notably, this smaller particle sizes of ZIF-8 provided a higher specific surface area and greater interaction with the external environment. Conversely, the larger particle sizes contributed to the formation of oversized pores, permitting the escape of AuNCs from ZIF-8 structure. Additionally, it retained a complete rhombic dodecahedral structure (Fig. 2E), with noticeable aggregations of AuNCs clearly visible within. To further investigate the distribution of AuNCs within the ZIF-8 framework, high-angle annular dark-field scanning TEM (HAADF-STEM) was employed to analyze the presence of corresponding elements (Fig. 2G). The results exhibited a uniform dispersion of Zn, N, Au, and S elements within the AuNCs@ZIF-8 nanostructure. This observation not only validated the existence of AuNCs within the ZIF-8 framework but also underscored that the introduction of AuNCs did not change the original morphology of ZIF-8.

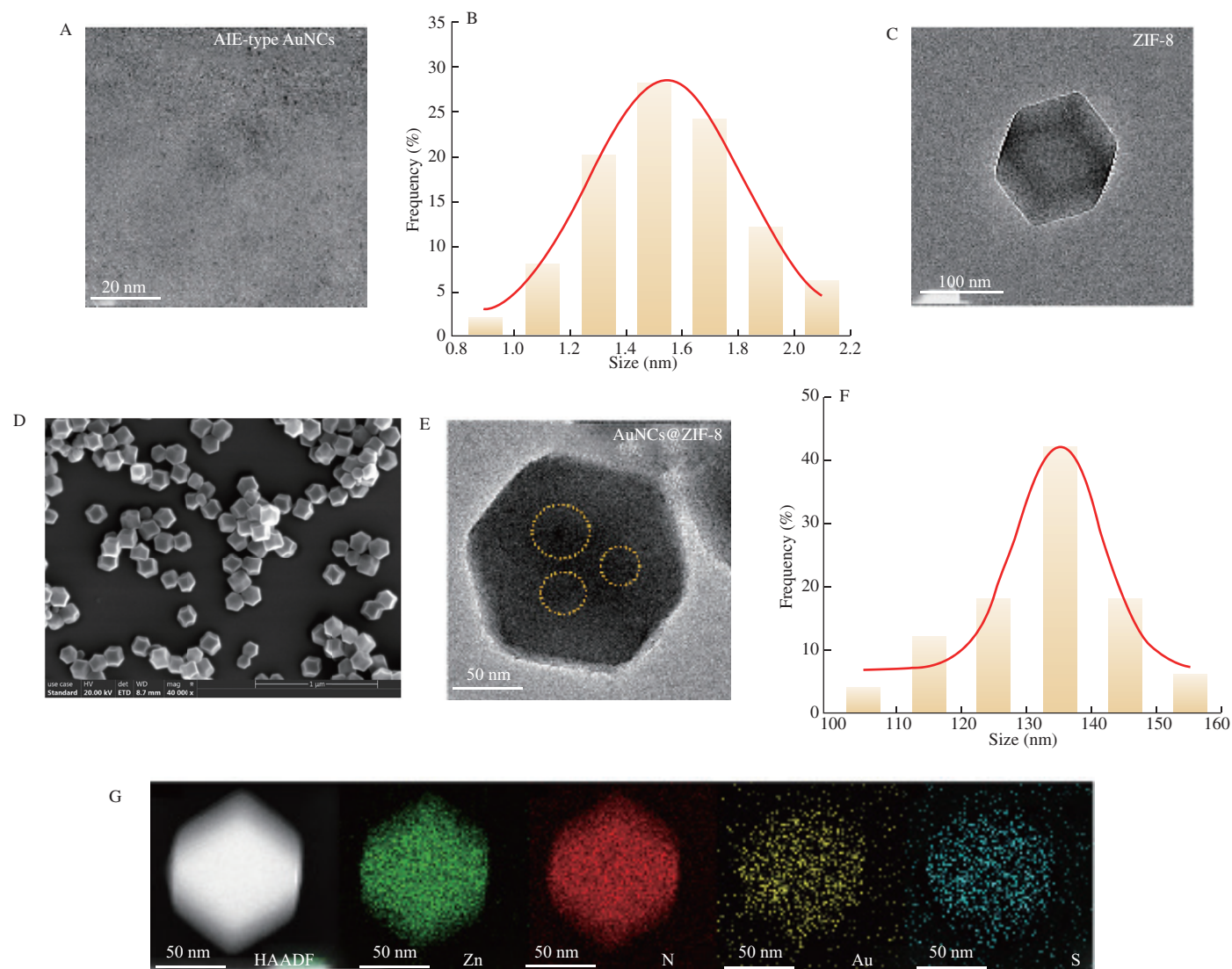
XRD was employed to investigate the crystal structure and composition of AuNCs@ZIF-8 nanocomposite. In Fig. 3A, characteristic peaks for the (011), (002), (112), (022), (013), (222), (114), (233), (134), (044), and (244) crystal planes of typical ZIF-8 were noted at corresponding  $2\theta$  values of  $7.38^\circ$ ,  $10.45^\circ$ ,  $12.82^\circ$ ,  $14.83^\circ$ ,  $16.61^\circ$ ,  $18.17^\circ$ ,  $22.27^\circ$ ,  $24.59^\circ$ ,  $26.84^\circ$ ,  $29.77^\circ$ , and  $30.69^\circ$ , respectively. Additionally, distinct diffraction peaks of AuNCs@ZIF-8 appeared at  $2\theta$  values of  $7.43^\circ$ ,  $10.51^\circ$ ,  $12.85^\circ$ ,  $14.85^\circ$ ,  $16.58^\circ$ ,  $18.17^\circ$ ,  $22.23^\circ$ ,  $24.62^\circ$ ,  $26.80^\circ$ ,  $29.77^\circ$ , and  $30.72^\circ$ , demonstrating structural similarity with ZIF-8 and indicating that the encapsulation of AuNCs did not affect the crystal structure growth of ZIF-8. The slight shifts observed in the characteristic peaks implied minor alterations in lattice distances after modification. Fig. 3B displayed the FT-IR results of AuNCs@ZIF-8 and ZIF-8. Both materials exhibited broad absorption bands within the range of  $3000\text{--}3300\text{ cm}^{-1}$  primarily attributed to  $\text{--OH}$  bonds. In pure ZIF-8, the bands at  $2927$  and  $3130\text{ cm}^{-1}$  were assigned to C–H stretching in the aromatic and aliphatic groups of imidazole, respectively, while bands at  $1308$  and  $1581\text{ cm}^{-1}$  corresponded to the stretching vibrations of the C–N and C=N groups. Characteristic peaks of stretching vibrations of the imidazole

rings were found in the spectral region  $600\text{--}1500\text{ cm}^{-1}$ , alongside a distinctive band at  $421\text{ cm}^{-1}$  attributed to Zn–N stretching, characteristic of the ZIF-8 structure. Notably, the presence of a distinct Zn–O peak at  $525\text{ cm}^{-1}$  in the AuNCs@ZIF-8 spectrum indicated that the formation of AuNCs@ZIF-8 relied on the coordination between  $\text{Zn}^{2+}$  ions and  $\text{--COO}^-$  in GSH. Furthermore, the elemental charge states were investigated through XPS experiments. As illustrated in Fig. 3C, the measured spectrum of the AuNCs@ZIF-8 nanocomposite exhibited 6 prominent peaks around Au 4f, S 2p, C 1s, N 1s, O 1s, and Zn 2p, confirming the presence of significant elements, including Zn, O, C, N, S, and Au in AuNCs@ZIF-8. High-resolution XPS spectra for Au and Zn (Figs. 3D and E) revealed specific features. The Au 4f spectrum of AuNCs@ZIF-8 showed 2 peaks at  $88.0$  and  $84.0\text{ eV}$ , corresponding to Au  $4f_{5/2}$  and Au  $4f_{7/2}$  of AuNCs, and The Zn 2p and Zn 3p spectrum had 2 peaks at  $1044.65$ ,  $1021.55$  and  $97.15$ ,  $89.05\text{ eV}$ , respectively, corresponding to Zn  $2p_{1/2}$ , Zn  $2p_{3/2}$  and Zn  $3p_{1/2}$ , Zn  $3p_{3/2}$  of AuNCs.

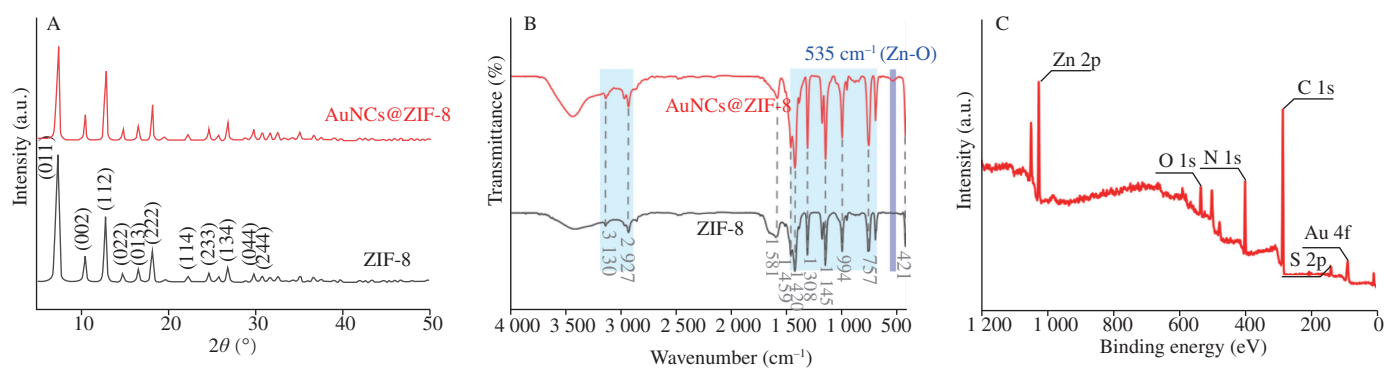
The  $\text{N}_2$  isothermal adsorption-desorption curves of AuNCs@ZIF-8 and ZIF-8 (Figs. S2A and B) both exhibited typical type I isotherms, indicative of their characteristic microporous structures and robust adsorption capacities. The encapsulation of AuNCs led to a specific surface area of  $1779.18\text{ m}^2/\text{g}$  and a pore volume of  $0.425\text{ m}^3/\text{g}$  for the prepared AuNCs@ZIF-8 nanocomposite, slightly lower than those of pure ZIF-8 ( $1947.03$ ,  $0.714\text{ m}^3/\text{g}$ ). Using density functional theory (DFT), the average micropore sizes of AuNCs@ZIF-8 and ZIF-8 were determined to be  $2.38$  and  $2.91\text{ nm}$ , respectively (Figs. S2C and D). These results indicated that the AuNCs@ZIF-8 nanocomposite maintained the microporous structure of ZIF-8, confirming that the AuNCs were encapsulated in ZIF-8 structure rather than being embedded in its pores. The TGA curves displayed in Fig. 3F demonstrated that the structure of ZIF-8 breakdown occurred at  $600^\circ\text{C}$ , correlating with a significant weight loss rate of  $71.92\%$ . Notably, this thermal decomposition temperature closely aligned with that of AuNCs@ZIF-8, which exhibited a weight loss rate of approximately  $84.11\%$ . This similarity in thermal decomposition temperatures suggested that the AuNCs@ZIF-8 nanocomposite inherited the high thermal stability characteristic of ZIF-8.

### 3.3 Optical properties and stability study of AuNCs and AuNCs@ZIF-8

The study conducted a comprehensive analysis of the optical properties of the prepared AuNCs and AuNCs@ZIF-8 materials. As illustrated in Fig. 4A, the UV spectra of the synthesized AIE-type AuNCs displayed a unique absorption peak at approximately  $400\text{ nm}$ , a typical feature distinguishing them from other AuNCs. Comparison of the UV absorption spectrum of ZIF-8 within the  $300\text{--}500\text{ nm}$  range showed a remarkable similarity with the spectra of the AuNCs@ZIF-8 nanocomposite. With an increase in the excitation wavelength ( $E_x$ ) ( $350\text{--}400\text{ nm}$ ), the emission wavelength ( $E_m$ ) of AuNCs@ZIF-8 remained constant (Fig. 4B). At an  $E_x$  of  $370\text{ nm}$ , the fluorescence intensity of AuNCs@ZIF-8 peaked at  $595\text{ nm}$ . Consequently, the optimal  $E_x$  and  $E_m$  of AuNCs@ZIF-8 were established at  $370$  and  $595\text{ nm}$ , respectively. Fig. 4C exhibited that pure ZIF-8 lacks an emission peak, contrasting sharply with the AuNCs@ZIF-8 nanocomposite, which displayed a distinct emission peak at  $595\text{ nm}$  with a fluorescence intensity approximately 7 times greater than that of the AuNCs at  $610\text{ nm}$ . This observation suggested that the fluorescence



**Fig. 2** TEM image (A) and size distribution diagram (B) of AuNCs; (C) TEM image of ZIF-8; SEM image (D), TEM image (E), particle size distribution (F), HAADF-STEM image and element mapping (N, Zn, Au, and S) (G) of AuNCs@ZIF-8.



**Fig. 3** (A) XRD spectra of AuNCs@ZIF-8 and ZIF-8; (B) FT-IR spectra of AuNCs@ZIF-8 and ZIF-8; (C) XPS spectrum of AuNCs@ZIF-8; XPS spectrum of (D) Au 4f and (E) Zn 2p for AuNCs@ZIF-8; (F) TGA spectra of AuNCs@ZIF-8 and ZIF-8.

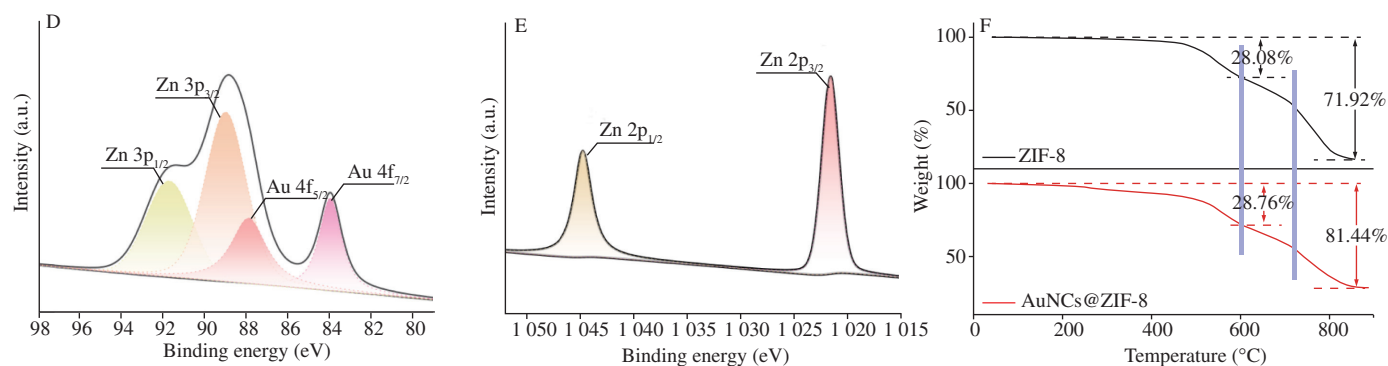


Fig. 3 (Continued)

from the AuNCs@ZIF-8 was derived from the encapsulated AuNCs, with the noted shift from 610 nm to 595 nm in  $E_M$  likely caused by the aggregation effects of AuNCs within ZIF-8 framework. The characteristic emission peaks of AuNCs in the supernatant at 400 nm almost disappeared after centrifugation of the AuNCs@ZIF-8 solution obtained from the reaction (Fig. S3), suggesting that the AuNCs were almost completely confined within the ZIF-8 framework. Furthermore, the fluorescence QY of the synthesized AuNCs and AuNCs@ZIF-8 materials were calculated to be 1.74% and 12.08%, respectively, using quinine sulfate (QS) as a reference (Fig. 4D).

The superior fluorescence properties of AuNCs were enhanced by the ZIF-8 framework, which also significantly improved their stability. Both the tolerance and storage stability of AuNCs@ZIF-8 under extreme conditions were investigated. Initially, both AuNCs@ZIF-8 and AuNCs underwent incubation at various temperatures (5–80 °C) for 1 h to assess their thermal resistance. As shown in Fig. 4E, following a 60 min heating period, the relative fluorescence intensity of AuNCs experienced a significant decrease as the temperature increased, contrasting with the relative fluorescence intensity of AuNCs@ZIF-8 remained essentially unchanged. Upon exposure to 365 nm UV irradiation for 60 min, the relative fluorescence intensity of AuNCs@ZIF-8 only decreased by 7.3% (Fig. 4F), further validating the superior stability conferred by ZIF-8 to AuNCs. Furthermore, Fig. 4G presented the fluorescence results of AuNCs and AuNCs@ZIF-8 solution after storage at 4 °C for 30 days. With the increase in storage time, there was a gradual decrease in the relative fluorescence intensity of AuNCs@ZIF-8, with it maintaining approximately 92.3% of its original value after 30 days. To assess the anti-photobleaching resistance, the relative fluorescence intensity of both was compared over 24 h, revealing a small enhancement in the anti-photostability of AuNCs with ZIF-8 encapsulation. This finding indicated that AuNCs@ZIF-8 exhibited higher reliability and longer lifespan under prolonged light exposure conditions. These results collectively demonstrated the remarkable stability of the AuNCs@ZIF-8 nanocomposite.

### 3.4 Conditions optimization for AuNCs@ZIF-8 synthesis

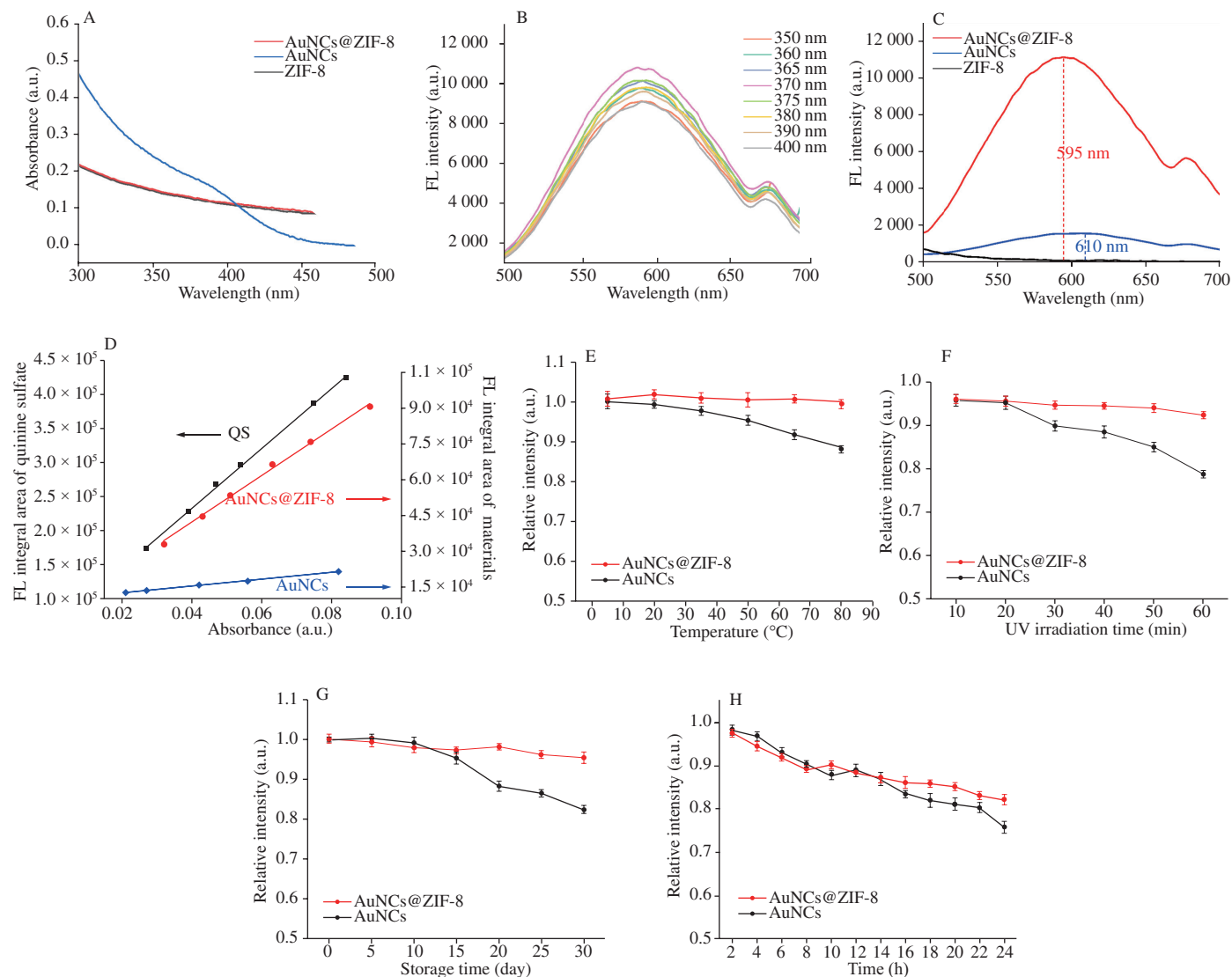
In order to optimizing the performance of the AuNCs@ZIF-8 nanocomposite, a detailed investigation into its preparation conditions was carried out. Organic solvents could induce the aggregation of the prepared AuNCs, thereby improving their encapsulation efficiency

during forming the ZIF-8 framework. As shown in Fig. S4A, by varying the proportion of ethanol in the system (0–100%), it was found that the color of AuNCs solution was significantly different under visible light and ultraviolet irradiation, and determined that a 50% ethanol content yielded the strongest fluorescence intensity, which was the optimal conditions for maximizing the intramolecular vibration and rotation of the ligands on the surface of the AuNCs. Consequently, a 50% ethanol system, achieved by mixing equal volumes of ethanol with the AuNCs preparation solution, was utilized to eliminate unreacted reactants. The dosage of AuNCs served as a crucial factor affecting the fluorescence performance of AuNCs@ZIF-8. As illustrated in Fig. S4B, increasing the amount of AuNCs from 1.0 mL to 4.0 mL led to a significant enhancement in fluorescence. However, an excessive amount of AuNCs (5.0 mL) resulted in incomplete encapsulation within the ZIF-8 framework and diminished the fluorescence intensity. Maintaining the integrity and stability of the ZIF-8 structure was greatly dependent on the amount of  $Zn^{2+}$  ions and 2-MI. It was observed that the highest fluorescence intensity was achieved for the AuNCs@ZIF-8 nanocomposite prepared with the addition of 2-MI (10.0 mL, 90 mmol/L) when the dosage of  $Zn^{2+}$  ions was 10.0 mL, 30 mmol/L. Fig. S4C illustrated the variation in fluorescence intensity of AuNCs@ZIF-8 over reaction time. A progressive enhancement in fluorescence of AuNCs@ZIF-8 intensity was discernible within the 10–40 min (Fig. S4D). However, beyond a 40 min incubation period, the thickness of the ZIF-8 shell impeded both photon transmission and excitation of AuNCs, consequently eliciting a decline in fluorescence intensity. Consequently, the experimental conditions for the synthesis of the AuNCs@ZIF-8 nanocomposite were determined as follows: 4.0 mL of AuNCs, along with a combination of  $Zn^{2+}$  ions (10.0 mL, 30 mmol/L) and 2-MI (10.0 mL, 90 mmol/L) reactants, were employed, with an incubation time of 40 min.

### 3.5 Conditions optimization for detecting glucose using AuNCs@ZIF-8 probe

The impact of microenvironmental pH on AuNCs and AuNCs@ZIF-8 nanocomposite was investigated in PBS at varying pH values (3.0–11.0). The mixed systems were incubated at 37 °C for 60 min and analyzed the fluorescence responses. As shown in Fig. 5A, while the fluorescence of the AuNCs was largely unaffected by changes in the microenvironmental pH, there was a significant alteration in





**Fig. 4** (A) UV-visible spectrum of AuNCs@ZIF-8, AuNCs and ZIF-8; (B) Fluorescence spectra of AuNCs at different  $E_x$ ; (C) Fluorescence emission spectra of AuNCs@ZIF-8, AuNCs and ZIF-8 ( $E_x$ : 370 nm); (D) The fluorescence QY of QS, AuNCs, AuNCs@ZIF-8; (E) Thermal stability of AuNCs@ZIF-8 and AuNCs at 5–80 °C; (F) Photostability of AuNCs@ZIF-8 and AuNCs under continuous irradiation at 365 nm for 10–60 min; (G) Fluorescence stability of AuNCs@ZIF-8 and AuNCs within 30 days; (H) Photobleaching resistance of AuNCs@ZIF-8 and AuNCs.

the fluorescence of the AuNCs@ZIF-8. Specifically, the  $\Delta F$  of the AuNCs@ZIF-8 remained relatively stable in neutral and alkaline environments but exhibited a sharp decrease in acidic conditions, decreasing by 42.6% at pH 5.0 compared to pH 7.0. TEM analysis revealed that the rhombic dodecahedral structure of ZIF-8 was disrupted in the incubated system, with AuNCs being released around the disassembled ZIF-8 and resuming free movement (Fig. 5B). Therefore, the breakdown of ZIF-8 weakened its confinement effects on AuNCs under acidic conditions, causing the “turn-off” of their AIE effects and resulting in a reduction in  $\Delta F$ . The pH sensitivity of AuNCs@ZIF-8 nanocomposite enabled the fluorescence behavior of AuNCs in the system to be synergistically regulated by pH and ZIF-8, providing a controllable mechanism for fluorescence detection.

As illustrated in Fig. 5C, separate mixtures of GOx and glucose with AuNCs@ZIF-8 were incubated at 37 °C for 60 min, resulting in nearly identical fluorescence spectra. However, upon their combination, a significant reduction in  $\Delta F$  was observed in the

AuNCs@ZIF-8 probe. This decrease was attributed to the catalytic action of GOx on glucose in the presence of oxygen, producing gluconic acid and  $H_2O_2$ , which reduced the system's pH. The reduction in  $\Delta F$  occurred due to the sensitivity of AuNCs@ZIF-8 to acidity. To achieve high analytical performance for the glucose targets, various parameters were adjusted while maintaining a constant glucose concentration of 10 mmol/L, including the PBS of pH, incubation time and temperature and the amount of GOx added. As illustrated in Fig. S5A, the significant change in  $\Delta F$  occurred at the PBS of pH at 6.5 which was chosen for experiments based on the stability and detection sensitivity of the AuNCs@ZIF-8. Upon adding a specific amount of GOx (4.5 U), the resulting  $\Delta F$  gradually increased with increasing incubation time from 10 to 30 min and tended to stabilize after 30 min (Fig. S5B). Combined with the optimal results of temperature (37 °C) and GOx amount (2.7 U) presented in Figs. S5C and D, the conditions for detecting glucose targets using the AuNCs@ZIF-8 probe were ultimately determined.



### 3.6 Detection of glucose using AuNCs@ZIF-8 probe

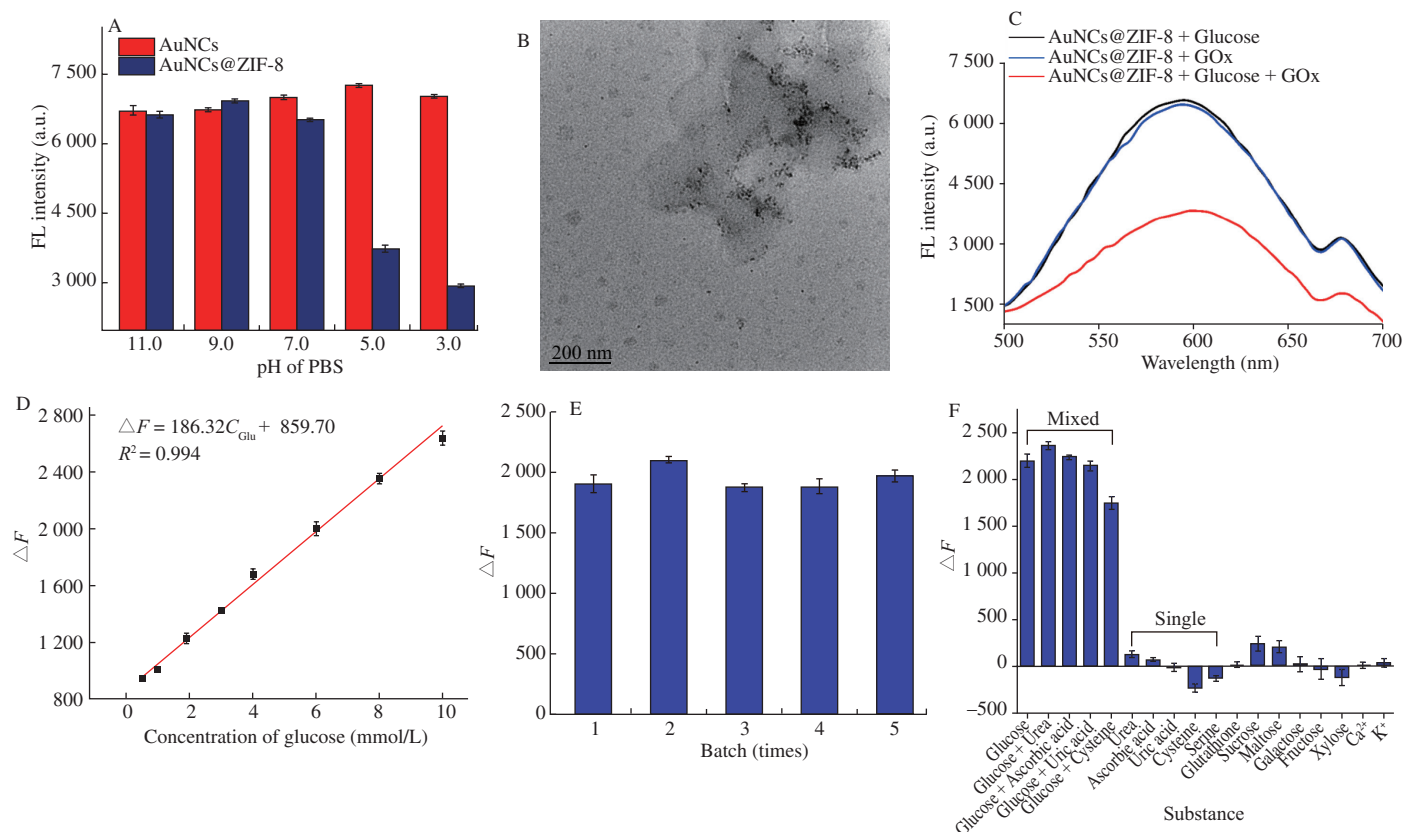
The glucose detection capability of the synthesized AuNCs@ZIF-8 probe was evaluated under optimal experimental conditions. As depicted in Fig. S6, the fluorescence emission spectra were recorded from the reaction system for varying concentrations of glucose solutions (0–10 mmol/L). Upon  $E_x$  at 370 nm, the  $\Delta F$  of the probe gradually decreased with the addition of glucose targets, accompanied by a slight red shift ( $E_m$ : 595–603 nm). The change in  $\Delta F$ , denoted as  $F(F_0 - F_i)$ , was determined by comparing the  $\Delta F$  at a glucose concentration of 0 mmol/L ( $F_0$ ) with that at a specific concentration ( $F_i$ ).

As the glucose targets concentration increased, there was a corresponding gradual increase in the  $\Delta F$  values, showing a strong linear relationship ( $R^2 > 0.99$ ) within the glucose concentrations range of 0.5–10 mmol/L (Fig. 5D). The LOD determined at a signal-to-noise ratio of 3 ( $S/N = 3$ ), was calculated to be 0.096 mmol/L. These findings demonstrated the precision, sensitivity, and usability of the designed AuNCs@ZIF-8 probe for detecting glucose targets. The relative standard deviation (RSD) of the fluorescence response  $\Delta F$  for 5 batches of prepared AuNCs@ZIF-8 probe to the same concentration of glucose solution (5 mmol/L) was only 2.1% ( $n = 3$ ), indicating excellent reproducibility and stability of the fluorescent probe throughout both preparation and application processes (Fig. 5E). The selectivity and interference resistance of the prepared AuNCs@ZIF-8 fluorescent probe for the glucose targets were further investigated.

As shown in Fig. 5F, comparing the  $F$  values of the glucose targets at a concentration of 5 mmol/L, even with concentrations of fructose, galactose, sucrose, xylose, and maltose up to 15 mmol/L at the same conditions,  $F$  values were insignificant. This depended on the good and specific catalysis of glucose by the GOx. Meantime, various potential interfering substances, including urea, uric acid, ascorbic acid, and cysteine (5 mmol/L), were introduced into the reaction system. The findings revealed that the performance of the AuNCs@ZIF-8 probe remained excellent, regardless of the presence of the target glucose (5 mmol/L). Additionally, the influence of other reducing substances (serine and GSH, 5 mmol/L) and inorganic ions ( $\text{Ca}^{2+}$  and  $\text{K}^+$ , 5 mmol/L), was assessed, with results showing they had little impact on  $\Delta F$ . Overall, the probe demonstrated outstanding specificity for glucose, providing accurate responses even in the presence of potential interferents.

### 3.7 Glucose analysis in real samples

The practical applicability of the prepared AuNCs@ZIF-8 fluorescent probe was evaluated by analyzing glucose levels in serums and glucose-containing beverages (Table 1). Fresh blood samples from 3 healthy volunteers were collected, centrifuged, and the resulting supernatant was analyzed for glucose content using the AuNCs@ZIF-8 probe. The results obtained an RSD of 2.0%–2.7% ( $n = 3$ ), and showed a correlation coefficient of 0.99 with those obtained from a commercial glucometer (Fig. S7A). In the evaluation



**Fig. 5** (A) Fluorescence intensity of AuNCs@ZIF-8 and AuNCs incubated in PBS at different pH for 1 h; (B) TEM image of AuNCs@ZIF-8 after incubation in PBS at pH 5.0 for 30 min; (C) Fluorescence spectra of AuNCs@ZIF-8 + glucose, AuNCs@ZIF-8 + GOx, and AuNCs@ZIF-8 + glucose + GOx; (D) Calibration curve of the  $\Delta F$  values of AuNCs@ZIF-8 versus glucose concentration; (E) Fluorescence response of AuNCs@ZIF-8 probe in 5 batches at concentrations of 5 mmol/L; (F) Fluorescence response to AuNCs@ZIF-8 probe of glucose (5 mmol/L), glucose structural analogues (15 mmol/L) and mixture of glucose and other substances (5 mmol/L).

of commercially available glucose beverages, the recoveries at 3 spiked concentrations (1.0, 4.0, and 7.0 mmol/L) fell within the range of 96.9%–104.3%, with an RSD of 1.8%–2.4% ( $n = 3$ ), and demonstrated a correlation coefficient surpassing 0.99 compared to results obtained from a glucose content kit (Fig. S7B). These results demonstrated the feasibility of the proposed AuNCs@ZIF-8 probe for the detection of glucose targets in real samples. Compared to other strategies for glucose analysis based on different principles

listed in Table 2, the proposed AuNCs@ZIF-8 probe demonstrated a broad linear range and a low LOD, providing reliable analytical results. Additionally, the detection process also offered significant cost advantages and did not require expensive and complex detection equipment. These advantages demonstrated the AuNCs@ZIF-8 probe presented an economical, sensitive, rapid, and convenient strategy for glucose quantification analysis.

**Table 1**

Detection results of glucose in serum and spiked beverages by AuNCs@ZIF-8 probe, glucometer method and glucose content kit method.

| Samples  |   | Initial concentration (mmol/L) | Spiked levels (mmol/L) | Total concentration (mmol/L) | AuNCs@ZIF-8 probe |              |                    | Glucometer method or glucose content kit method |              |
|----------|---|--------------------------------|------------------------|------------------------------|-------------------|--------------|--------------------|-------------------------------------------------|--------------|
|          |   |                                |                        |                              | Found (mmol/L)    | Recovery (%) | RSD (% , $n = 3$ ) | Found (mmol/L)                                  | Recovery (%) |
| Serum    | 1 | -                              | -                      | -                            | 5.06              | -            | 2.02               | 5.20                                            | -            |
|          | 2 | -                              | -                      | -                            | 6.31              | -            | 2.67               | 6.40                                            | -            |
|          | 3 | -                              | -                      | -                            | 5.26              | -            | 1.96               | 5.50                                            | -            |
| Beverage | 1 | 1.46                           | 1.0                    | 2.46                         | 2.54              | 107.86       | 2.04               | 2.39                                            | 93.46        |
|          |   |                                | 4.0                    | 5.46                         | 5.79              | 108.23       | 1.83               | 5.49                                            | 100.72       |
|          |   |                                | 7.0                    | 8.46                         | 8.70              | 103.42       | 3.22               | 8.55                                            | 101.30       |
|          | 2 | 2.06                           | 1.0                    | 3.06                         | 2.91              | 85.36        | 3.16               | 3.01                                            | 95.54        |
|          |   |                                | 4.0                    | 6.06                         | 5.87              | 95.36        | 2.48               | 6.18                                            | 103.42       |
|          |   |                                | 7.0                    | 9.06                         | 9.04              | 99.69        | 1.90               | 9.14                                            | 101.19       |
|          | 3 | 2.46                           | 1.0                    | 3.46                         | 3.38              | 92.24        | 3.19               | 3.52                                            | 106.09       |
|          |   |                                | 4.0                    | 6.46                         | 6.43              | 99.29        | 2.39               | 6.60                                            | 104.33       |
|          |   |                                | 7.0                    | 9.46                         | 9.53              | 101.05       | 2.32               | 9.63                                            | 102.36       |

Note: -, No spiked process in serum samples.

**Table 2**

Comparison of the proposed fluorescent probe with other reported glucose detection strategies.

| Methods                | Materials                                   | LOD (mmol/L) | Linear range (mmol/L) | Sample              | Reference |
|------------------------|---------------------------------------------|--------------|-----------------------|---------------------|-----------|
| SERS                   | Au@Ag NPs                                   | 0.1          | 0.1–6                 | Urine               | [30]      |
|                        | Au NPs/Cu-TCPP(Fe)                          | 0.004        | 0.16–8                | Salivary            | [9]       |
|                        | 4-MPBA/AgNP                                 | 0.1          | 1–10                  | Cell                | [31]      |
|                        | AgNP@cys/Au wafer@4-ATP                     | 0.5          | 0.5–8                 | Serum               | [32]      |
| Electrochemical        | ZnO: Co <sup>2+</sup>                       | -            | 1–7                   | -                   | [33]      |
|                        | Mn-NiO NSs/CC                               | 0.000 6      | 0.002–2.14            | Beverage            | [34]      |
|                        | PUC-PANI-ZnO@GOx                            | 0.007        | 0.01–9.48             | -                   | [35]      |
|                        | ExGCP                                       | 0.812        | 2–8                   | -                   | [36]      |
|                        | GOx/MnOxides/PE                             | 0.29         | 0.56–5.55             | Beverage            | [37]      |
|                        | MBE Grown VOx                               | 0.32         | 1–10                  | -                   | [38]      |
| Colorimetric           | MnO <sub>2</sub>                            | 0.01         | 0.01–5                | Serum               | [39]      |
|                        | Cu NSs-OPD-GOD                              | 0.005 5      | 0.01–5                | Beverage            | [40]      |
|                        | TiO <sub>2</sub> /I <sub>2</sub> /CMC (TIC) | 0.4          | 0.5–10                | -                   | [41]      |
| Paper-based analytical | GOx                                         | 0.4          | 0.5–10                | Glucose             | [42]      |
|                        | GOx-mediated sodium alginate gelation       | 1.4          | 1.4–7.0               | Fruit               | [43]      |
| Fluorescence           | BSPOTPE/BSA-AuNCs                           | 0.1          | 1–8                   | Serum               | [44]      |
|                        | APBA-CuInS <sub>2</sub> QDs                 | 0.001        | 0.005–8               | Serum               | [45]      |
|                        | N-CDs@ZnO                                   | 0.25         | 1–6                   | Serum and blood     | [46]      |
|                        | BG-PAA/GOx                                  | 0.055        | 0.25–5                | Beverage            | [47]      |
|                        | Au NCs@FGO                                  | 0.16         | 1–10                  | Serum               | [48]      |
|                        | AuNCs@ZIF-8                                 | 0.096        | 0.5–10                | Serum and beverages | This work |

Note: 4-MPBA, 4-Mercaptophenylboronic acid. Cu-TCPP(Fe), Cu-tetra (4-carboxyphenyl) porphyrin chloride (Fe (III)). CC, Carbon cloth. PUC, Polyurethane-chitosan. ExGCP, exfoliated graphite carbon paper. PE, pencil graphite electrode. MBE, molecular beam epitaxy. BSPOTPE, 1,2-bis[4-(3-sulfonatopropoxy)phenyl]-1,2-diphenylethane. APBA, 3-aminophenylboronic acid. BG-PAA, brilliant-green sequestered poly (amic) acid. FGO, fluorescent graphene oxide.

## 4. Conclusions

In this study, a highly fluorescent AuNCs@ZIF-8 nanocomposite was successfully developed by capitalizing on the “AIE” effects of AuNCs and the domain-limiting effects provided by ZIF-8. Furthermore, the acidic environment resulting from GOx catalysis on glucose was utilized to induce the structural decomposition of ZIF-8, diminishing the confinement around AuNCs, preventing their aggregation, and facilitating accurate and rapid detection of glucose. The resulting pH-responsive fluorescent probe is not only simple to prepare and store but also highly accurate and rapid, providing an effective strategy for quantifying glucose levels in clinical samples and beverages. Future research may explore potential applications of this pH-responsive fluorescent probe across various fields.

## Declarations of competing interests

Shuo Wang is an editorial board member for *Food Science and Human Wellness* and was not involved in the editorial review or the decision to publish this article. The authors declare no competing financial interest.

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## Appendix A. Supplementary data

Supplementary data associated with this article can be found, in the online version, at <http://doi.org/10.26599/FSHW.2024.9250392>.

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